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KARLA SHANGELA DA SILVA ALVES

**EFEITO DO PLASMA DE BAIXA TEMPERATURA E PRESSÃO NO BIOFILME ORAL
FORMADO SOBRE ESMALTE EM UM MODELO *IN SITU***

FORTALEZA

2016

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Tese apresentada ao Programa de Pós-Graduação em Odontologia da Faculdade de Farmácia, Odontologia e Enfermagem da Universidade Federal do Ceará, como requisito parcial para obtenção do título de Doutor em Odontologia. Área de concentração: Clínica Odontológica.

Orientadora: Profa. Dra. Iriana Carla Junqueira Zanin dos Santos.

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Aprovada em ___ / ___ / ___

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(Valdemir Antoneli)

RESUMO

O plasma de baixa temperatura é uma tecnologia promissora que vem sendo estudada na odontologia por suas várias propriedades, dentre elas, por sua capacidade de destruir bactérias presentes em biofilme maduro destruindo a matriz do biofilme oral. O objetivo deste estudo foi avaliar o potencial antimicrobiano do plasma de argônio de baixa temperatura em biofilmes orais formados *in situ* e verificar se o tratamento proposto danifica a estrutura do esmalte tratado. Para tanto, vinte e dois voluntários utilizaram dispositivos intraorais palatinos contendo 6 blocos de esmalte bovino que foram gotejados sacarose 10 vezes ao dia uma solução de sacarose a 10%, durante 7 dias. Ao final do período intraoral, os biofilmes formados sobre os blocos de esmalte receberam tratamento durante 5 minutos com plasma de argônio, gás argônio, clorexidina a 0,12%, ou solução salina de NaCl a 0,89%. As amostras dos biofilmes foram coletadas, pesadas, diluídas de forma seriada e plaqueadas em meio de cultivo para o crescimento de microrganismos totais, estreptococos totais, estreptococos do grupo *mutans* e lactobacilos. A fim de analisar se os tratamentos danificaram a estrutura do esmalte, os blocos foram analisados por microscopia eletrônica de varredura (MEV) e por espectroscopia Raman. O tratamento do plasma mostrou uma redução significativa na viabilidade dos microrganismos totais ($p < 0,001$), estreptococos totais ($p = 0,037$) e estreptococos do grupo *mutans* ($p = 0,004$). O gás de argônio também reduziu significativamente as contagens de estreptococos do grupo *mutans*. O tratamento com plasma não demonstrou influência sobre a viabilidade dos lactobacilos nas condições testadas ($p = 0,497$). A MEV revelou regiões lisas e homogêneas na superfície do esmalte, não sendo observadas diferenças topográficas entre os esmaltes sob biofilmes submetidos aos diferentes tratamentos. No Raman, foram identificadas quatro bandas principais presentes na fase inorgânica: 324 (V1), 582 (V2), 960 (V3) e 1045 (V4) cm^{-1} e outras 4 identificadas na fase orgânica 1448 (V5), 1465 (V6), 1653 (V7) 2943(V8) cm^{-1} , não ocorrendo diferenças estatísticas entre os espectros do Raman nos blocos de esmaltes dos diferentes tratamentos. Em conclusão, o plasma foi eficaz na redução de bactérias viáveis presentes em biofilmes orais maduros produzidas *in situ* e não alterou a superfície do esmalte sob biofilme tratado.

Palavras-chaves: Placa dentária. Gases em plasma. Agentes antimicrobianos.

ABSTRACT

The Low temperature plasma is a promising technology that has been studied in dentistry for its various properties, among them, for their ability to destroy bacteria present in mature biofilm and also destroying the polymeric matrix of oral biofilms. The aim of this study was to evaluate the antimicrobial effect of argon plasma on oral biofilms formed *in situ* and also verify if this treatment damages the structure of the treated enamel. For that, twenty-two volunteers used palatine intraoral devices containing 6 to bovine enamel slabs that were dripped sucrose 10 times a day with 10% sucrose. The intraoral period was 7 days. At the 7th day, enamel slabs were treated for 5 minutes with plasma, argon flow, 0.12% chlorhexidine, or 0.89% NaCl solution. Thus, biofilms samples were collected, weighed, serially diluted and plated in culture medium for the growth of total microorganisms, total streptococci, *mutans streptococci* and *lactobacilli*. In order to analyze whether the treatments damaged the enamel structure, the slabs were analyzed by scanning electron microscopy (SEM) and Raman spectroscopy. Low temperature plasma treatment showed a significant reduction in the viability of the total microorganisms ($p < 0.001$), total streptococcus ($p = 0.037$) and *mutans streptococci* ($p = 0.004$). Argon flow also significantly reduced the *mutans streptococci* counts. The plasma treatment did not influence on the viability of the *lactobacilli* under the conditions tested ($p = 0.497$). SEM revealed smooth and homogeneous regions on the enamel surface, unobserved topographical differences between the glazes in biofilms subjected to different treatments. In Raman spectroscopy, we identified four major bands present in the inorganic phase: 324 (V1), 582 (V2), 960 (V3) e 1045 (V4) cm^{-1} and other 4 identified in the organic layer 1448 (V5), 1465 (V6), 1653 (V7) 2943(V8) cm^{-1} . No statistical differences in the Raman spectra were observed for enamel of different treatments. In conclusion, the plasma was effective in reducing viable bacteria present in mature oral biofilms produced *in situ* and not alter in the enamel surface treated biofilms.

Keyword: Dental Plaque. Plasma Gases. Anti-Infective Agents.

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LISTA DE ABREVIATURAS E SIGLAS

AIR	<i>Argon flow</i>
Caae	Certificado de apresentação para apreciação ética
CAPES	Coordenação de Aperfeiçoamento de Pessoal de Nível Superior
CFU	<i>Colony-Forming Units</i>
CHX	<i>Chlorhexidine</i>
cm	Centímetros
DNA	Ácido desoxirribonucleico
F	Flúor
FM	<i>Future-Tech</i>
KV	Quilovolt
MEV	Microscópio Eletrônico de Varredura
min	Minuto
mm	Milímetro
MSA	<i>Mitis Salivarius Agar</i>
MSB	<i>Mitis Salivarius Bacitracina</i>
NaCl	Cloreto de sódio
nm	Nanômetro
PLA	Plasma
SAL	<i>Salina solution</i>
SD	<i>Standard Deviation</i>
SEM	<i>Scanning Electron Microscopy</i>
SMH	<i>Surface Microhardness</i>
SMHC	<i>Surface Microhardness Change</i>
TTP	<i>Tissue-Tolerable Plasma</i>
V	Volt
μL	Microlitros
μm	Micrometro

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1 INTRODUÇÃO

A grande maioria dos microrganismos na natureza encontra-se ligada às superfícies, onde crescem na forma de biofilmes. Os biofilmes bacterianos são formados quando microrganismos unicelulares se tornam irreversivelmente aderidos a uma superfície sólida e envolvida por uma matriz de polissacarídeos extracelulares, podendo haver a formação de biofilmes a partir de uma ou de múltiplas espécies bacterianas (MAH & O'TOOLE, 2001, p. 34). Tem sido observado que bactérias inseridas nos biofilmes passam a exibir características fenotípicas distintas, as quais resultam no aumento de sua resistência aos agentes antimicrobianos de modo que essas comunidades microbianas têm grande importância em ambientes clínicos, ambientais e industriais (O'TOOLE, 2016, p. 5).

A placa dentária é um biofilme dinâmico composto por um ecossistema microbiano formado por centenas de espécies que se acumulam sobre a superfície dos dentes (FILOCHE, WONG, SISSONS, 2010, p. 10). O biofilme oral é único entre os vários tipos de biofilmes (HUANG, LI, GREGORY, 2011, p. 436) por requerer glicoproteínas salivares para anexar ao substrato. É composto por estruturas tridimensionais complexas, formado por comunidades de multi-espécies microbianas sobre o tecido oral (HE *et al.*, 2015, p. 70), incorporados em uma matriz de polissacarídeos extracelulares (EPS) (HOJO *et al.*, 2009, p. 983; YANG *et al.*, 2011, p. 74).

O primeiro passo na formação do biofilme oral é a ligação da película adquirida, uma fina camada de glicoproteínas de origem salivar ou bacteriana que se adere à superfície dentária. Logo em seguida, inicia-se a adesão bacteriana com as bactérias pioneiras. *Actinomyces spp*, *Streptococcus spp*, *Haemophilus spp*, *Capnocytophaga spp*, *Veillonella spp*, *Neisseria* são os principais gêneros de bactérias pioneiras a aderir à superfície do dente (DIGE *et al.*, 2009, p. 70; HUANG, LI, GREGORY, 2011, p. 437). Ao longo do tempo, a diversidade bacteriana do biofilme cresce (RICKARD *et al.*, 2003, p. 96), as bactérias pioneiras fornecem locais de ligações específicos às bactérias subsequentes e promovem o desenvolvimento do biofilme que aumenta gradualmente em espessura e em complexidade com a maturação da placa (HUANG, LI, GREGORY, 2011, p. 437).

Um número estimado de 700 espécies bacterianas, incorporadas em matriz rica em polissacarídeo extracelular, foram encontradas dentro do biofilme oral (KOO, FALSETTA, KLEIN, 2013, p. 1070; NIKITKOVA, HAASE, SCANNAPIECO, 2013, p. 420). As bactérias em biofilmes mostram uma virulência mais elevada em comparação a seus homólogos planctônicos (HOJO *et al.*, 2009, p. 983), podendo ser de 10 a 1000 vezes mais resistentes às terapias antimicrobianas convencionais com agentes antibacterianos, como a clorexidina ou

os antibióticos (WELIN-NEILANDS; SVENSÄTER, 2007, p. 5635; KARYGIANNI *et al.*, 2014b, p. 7330). Ocorre, no entanto, que o uso frequente desses agentes no tratamento de doenças crônicas pode resultar no desenvolvimento de resistência por algumas espécies, o que se tornou um problema de saúde pública mundial (SMITH *et al.*, 2013, p. 584).

Recentemente, grandes esforços têm sido colocados na pesquisa odontológica a fim de encontrar novos métodos para eliminar microrganismos patogênicos presentes nos biofilmes orais (KARYGIANNI *et al.*, 2016, p. 1) que não resultem no surgimento de cepas resistentes. Neste contexto, surgem os plasmas de baixa temperatura (PBT) para o tratamento antimicrobiano, sendo uma tecnologia alternativa de grande potencial e uma ferramenta promissora em uma variedade de aplicações biomédicas, com particular importância para combater infecções (MAI-PROCHNOWA *et al.*, 2014, p. 508) por inativar bactérias (ERMOLAEVA *et al.*, 2011, p. 80), fungos (FRICKE *et al.*, 2012, p. 438; KLAMPFL *et al.*, 2012, p. 5077), esporos (VENEZIA *et al.*, 2008, p. 43), parasitas (ERMOLAEVA *et al.*, 2012 p. 793) e vírus (ALSHRAIEDEH *et al.*, 2013, p. 1420).

Os plasmas, que podem ser definidos como o quarto estado da matéria, são formados a partir da ionização de gases como: argônio, hélio, ozônio ou gás oxigênio. É constituído por partículas em interação permanente que incluem fótons, elétrons, íons positivos e negativos, átomos, radicais livres e moléculas excitadas e não excitadas (MOREAU; ORANGE; FEUILLOLEY, 2008, p. 611). Em geral, existem dois tipos de plasma gasoso, o plasma térmico e o não térmico. Os plasmas térmicos são obtidos a alta pressão (≥ 105 Pa), precisam de uma potência maior para serem formados (até 50 MW), possuem elétrons e partículas pesadas à mesma temperatura, isto é, eles estão em equilíbrio térmico entre si. Os plasmas não térmicos ou de baixa temperatura são obtidos a baixas pressões e potências sendo caracterizados por uma temperatura muito elevada dos elétrons mais do que a do gás (temperatura macroscópica), enquanto os íons e os átomos neutros são obtidos a uma temperatura muito menor (normalmente temperatura ambiente) e conseqüentemente não apresentam um equilíbrio termodinâmico local (MAI-PROCHNOWA *et al.*, 2014, p. 508; SCHOLTZ *et al.*, 2015, p. 58). Um plasma é às vezes chamado de "quente" se ele está quase totalmente ionizado ou "frio" se apenas uma pequena fração (por exemplo, 1%) das moléculas do gás estão ionizadas (MOREAU; ORANGE; FEUILLOLEY, 2008, p. 612).

As vantagens do PBT sobre outros agentes antimicrobianos são que ele pode ser usado para um tratamento localizado, fornecendo uma resposta bactericida instantânea (segundos de aplicação), o que torna a probabilidade do desenvolvimento de resistência bacteriana ao PBT baixa, e a terapia tem demonstrado efeitos colaterais mínimos. Além disso, a temperatura do PBT é compatível com os tecidos das células mamárias, o que incentiva a sua utilização *in*

vivo (FLUHR *et al.*, 2012, p. 130, PARTECKE *et al.*, 2012, p. 1). Espécies reativas são geradas transitoriamente pelo PBT através de diversas vias de colisões e dissociações. Estas espécies reativas oxidantes têm fortes efeitos sobre as estruturas externas das células, seja um revestimento de esporos ou de uma membrana celular. As gorduras insaturadas na bicamada lipídica das membranas celulares são susceptíveis ao ataque por radicais de hidroxila, comprometendo a função da membrana e as proteínas em membranas. Os revestimentos dos esporos são susceptíveis ao dano oxidativo por ataque químico pelas espécies reativas. Uma vez que a membrana celular e os revestimentos dos esporos foram parcialmente degradados, as espécies reativas podem danificar o material genético e as moléculas dentro do microrganismo, levando a sua destruição (HOFFMANN; BERGANZA; ZHANG, 2013, p. 21; MAI-PROCHNOWA *et al.*, 2014, p. 508; SCHOLTZ *et al.*, 2015, p. 53).

Adicionalmente, os tratamentos com PBTs para várias aplicações biomédicas e médicas, incluindo cicatrização de feridas, não mostraram efeitos adversos e forneceram provas da segurança da tecnologia (FLUHR *et al.*, 2012, p. 130). Pesquisas têm demonstrado que o tratamento com o plasma a baixa temperatura (PBT) pode matar bactérias orais (YAMAZAKI *et al.*, 2011, p. 390; GORYNIA *et al.*, 2013, p. 1; BLUMHAGEN *et al.*, 2014, p. 89) e inibir completamente a formação de um biofilme rico em matriz (DUARTE *et al.*, 2011, p. 1).

Vários autores têm estudado as possíveis utilidades do PBT no campo da odontologia: no clareamento dentário (LEE *et al.*, 2010, p. 240; SUN *et al.*, 2010, p. 1892; JIE *et al.*, 2010, p. 3143; PARK *et al.*, 2011, p. 170; SEOUL *et al.*, 2013, p. 265), na esterilização de instrumental (RUPF *et al.*, 2012, p. 126; KOBAN *et al.*, 2011, p. 956; SU-JIN *et al.*, 2013, p. 2; IDLIBI *et al.*, 2013, p. 369) e na adesão das restaurações a dentina (RITTS *et al.*, 2010, p. 510, HIRATA *et al.*, 2016, p.215). Além disso, diversos autores testaram a ação antimicrobiana do plasma em biofilmes *in vitro* bacterianos de *S. mutans* (GOORE *et al.*, 2006, p. 1317), *B. cereus* e *G. Stearothermophilus* (MORRIS *et al.*, 2009, p. 55), *L. acidophilus* e *S. mutans* (BO *et al.*, 2011, p. 48), *P. Gingivalis* (MAHASNEH *et al.*, 2011, p. 191), *S. mutans* (SUN *et al.*, 2011, p. 143702) e em canais radiculares (JIANG *et al.*, 2009, p. 479; LU *et al.*, 2009, p. 668; SHAUDINN *et al.*, 2013, p. 1).

Assim, a tecnologia do PBT tem recebido crescente atenção como uma possível terapia para o tratamento e/ou prevenção de biofilmes. Muitos estudos sugerem a terapia com PBT um importante agente antibacteriano, mas relatam terapias utilizando uma variedade de diferentes dispositivos geradores de plasma com diferentes tipos de gases e tempo de tratamentos dos biofilmes diferentes, o que torna um desafio mostrar a reprodutibilidade dos resultados. Em contraste com seu efeito antimicrobiano, ainda não se tem conhecimento de

como o PBT afeta a estrutura do esmalte. Além disso, é necessário determinar parâmetros seguros para a utilização do PBT nos tecidos dentais antes que o mesmo seja recomendado para o uso clínico. Até esta data, tem havido algumas investigações em relação ao tratamento de bactérias orais com PBT (BIN *et al.*, 2006, p. 1317; SLADEK *et al.*, 2007 p. 318; YAMAZAKI *et al.*, 2011, p. 384; GORYNIA *et al.*, 2013, p. 1; BLUMHAGEN *et al.*, 2014, p. 84; SLADEK *et al.*, 2014), mas não há estudos com biofilmes formados *in situ*, de modo a investigar a terapia sob condições mais próximas àquelas encontradas na cavidade bucal dos seres humanos.

2 PROPOSIÇÃO

Avaliar o potencial antimicrobiano do plasma de argônio de baixa temperatura em biofilmes orais formados *in situ* e os seus possíveis efeitos na morfologia e composição química do esmalte bovino sob o biofilme irradiado.

3 CAPÍTULO

Esta tese está baseada no Artigo 46 do Regimento Interno do Programa de Pós-Graduação em Odontologia da Universidade Federal do Ceará, que regulamenta o formato alternativo para dissertação de mestrado e tese de doutorado e permite a inserção de artigos científicos de autoria e coautoria do candidato. Por se tratar de pesquisa envolvendo seres humanos, ou parte deles, o projeto de pesquisa deste trabalho foi submetido à apreciação do Comitê de Ética em Pesquisa da Faculdade de Medicina da Universidade Federal do Ceará via Plataforma Brasil, tendo sido aprovado sob Caae - 40975514.0.0000.5054 (ANEXO A). Assim sendo, essa tese de doutorado é composta de um capítulo que contém um artigo que será submetido para publicação no periódico “Caries Research” (ANEXO B).

3.1 Capítulo 1

Effect of tissue-tolerable plasma on oral biofilms formed *in situ*. Karla Shangela da Silva Alves, Roberto Haniery Pontes Alves, Ramille Araújo Lima, Maria Silmara Alves de Santana, Lidiany K. A. Rodrigues, Simone Duarte, Iriana C. J. Zanin.

Title: Effect of Tissue-Tolerable Plasma on oral biofilms formed *in situ*.

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1 ABSTRACT

2 The Tissue-Tolerable Plasma - TTP is a promising technology that has being studied in
3 dentistry due to not only its ability to kill bacteria present in mature biofilm and but also to
4 destroy the polymeric matrix of oral biofilms. The aim of this study was to evaluate the
5 antimicrobial effect of argon TTP on oral biofilms formed *in situ* and also verify if this
6 treatment damages the structure of enamel under treated biofilm. For that, twenty-two
7 volunteers used palatine intraoral devices containing bovine enamel slabs that were
8 treated 10 times per day with a 10% sucrose. After a 7 day intraoral period, the biofilm
9 formed over the enamel slabs were treated for 5 minutes, as follows: TTP, argon flow,
10 0.12% chlorhexidine, or 0.89% NaCl solution. Thus, biofilms samples were collected,
11 diluted in decimal series and plated in culture medium for the growth of total
12 microorganisms, total streptococci, *mutans streptococci* and *lactobacilli*. In order to
13 analyze whether the treatments damaged the enamel structure, the slabs were analyzed
14 by scanning electron microscopy (SEM) and Raman spectroscopy. Tissue tolerable
15 plasma treatment showed a significant reduction in the viability of the total microorganisms
16 ($p < 0.001$), total streptococcus ($p = 0.037$) and *mutans streptococci* ($p = 0.004$). Argon flow
17 also significantly reduced the *mutans streptococci* counts. The plasma treatment did not
18 influence on the viability of the lactobacilli under the conditions tested ($p = 0.497$). SEM
19 revealed smooth and homogeneous regions on the surface of the treated enamel,
20 unobserved topographical differences between the enamel subjected to different
21 treatments. In Raman spectroscopy, we were identified four major bands present in the
22 inorganic phase: 324 (V1), 582 (V2), 960 (V3) e 1045 (V4) cm^{-1} and other 4 identified in
23 the organic layer 1448 (V5), 1465 (V6), 1653 (V7) 2943(V8) cm^{-1} . No statistical differences
24 in the Raman spectra were observed for enamel of different treatments. In conclusion, the
25 plasma was effective in reducing viable bacteria present in mature oral biofilms produced
26 *in situ* and it did not modify the morphology and composition the enamel.

27

28 INTRODUCTION

29 Biofilms models may help us to accurately predict, in a controlled and simplified
30 way, a clinical outcome which can lead us to preventive actions for diseases
31 [Featherstone, 1996]. One example of biofilm model is the *in situ* biofilm, which may be
32 formed on different substrates that are introduced inside the oral cavity into oral devices.
33 Several models, which enable the development of non-disturbed oral biofilm, are found in
34 literature. The first report was done by Ahrens et al. [1976] and they developed a model
35 based on acrylic splints on which enamel slides were positioned. Since then, this system
36 has been widely used with a variety of substrates including glass [Arweiler et al., 2004],
37 bovine enamel [Jentsch et al., 2002], bovine dentin [Zaura-Arite et al., 2001], human
38 enamel [Teixeira et al., 2012] and dentin [Lima et al., 2009] and hydroxyapatite discs
39 [Sreenivasan et al., 2009].

40 Antimicrobial agents are used due its ability to avoid dental biofilm formation, but
41 biofilm species may exhibit several resistance mechanisms against them [Mah&O'Toole
42 2001]. In addition, the age and the structure of a biofilm may also restrict the penetration of
43 the antimicrobial agent and deeper cells in the biofilm could not be affected [Zanin et al.,
44 2005]. Disruption of the oral microflora and the difficulty of maintaining therapeutic
45 concentrations of antimicrobials in the oral cavity are also problems associated with its
46 usage [Zaura-Arite et al., 2001]. Thus an antimicrobial adjuvant would be a valuable
47 alternative in treating oral infections.

48 Regarding these alternative adjuvants, Tissue-Tolerable Plasma - TTP, that
49 represents the fourth state of matter after solid, liquid, and gaseous [Morfill et al., 2009],
50 emerges as an alternative once it is a technology that inhibits biofilm formation with the
51 potential benefit of destroying oral biofilm matrix [Duarte et al., 2011]. Plasma is a partially
52 ionized gas generated by an electrical discharge, which creates a highly reactive
53 environment with ions, electrons, excited atoms and molecules, vacuum ultraviolet and
54 ultraviolet irradiation, free radicals and chemically reactive particles [Koban et al., 2010;
55 Zamperini et al., 2010]. The production of stable plasma at atmospheric pressure has
56 attracted attention for treating living cells and tissues without thermal damage [Brun et al.,
57 2012]. It is also site specific, targeting only the infected area [Goree et al., 2006], and it
58 seems to preserve the material's bulk properties [Zamperini et al., 2010]. In addition,
59 plasma is usually produced by low-toxicity gases and elaborates its activity by producing a
60 mixture of products that decay within a few seconds after the treatment process.

61 Therefore, this approach has been suggested as environmentally friendly with no harmful
62 residues [Alkawareek et al., 2012].

63 TTP has recently been extensively studied by researchers as a possible therapy in
64 dentistry. Researchers have mostly investigated the antimicrobial effects produced by
65 plasma as a means to remove dental biofilms and eradicate oral pathogens. It has been
66 shown that antimicrobial effects the TTP are carried out by induction reactive, photons and
67 reactive particles, ions, and molecules [Hasse et al., 2015]. The efficacy of TTP against an
68 extended spectrum of fungi and bacteria, including *S. mutans*, has been shown in several
69 *in vitro* studies [Rupf et al., 2010; Matthes et al., 2013; Bender and Kramer, 2014;
70 Preissner et al., 2015], but no studies report results in multispecies biofilms. Furthermore,
71 it has been applied effectively in antimicrobial therapy in case reports and clinical studies
72 in animals and humans, especially in otorhinolaryngology and dermatology [Isbary et al.,
73 2013; Klebes et al., 2015]. Strikingly, its efficacy seems to be irrespective of microbial
74 resistance patterns [Haertel et al., 2014; Daeschlein et al., 2015] and no negative side
75 effects to viable tissues have been described, despite slight warming and temporary
76 redness [Lademann et al., 2009; Fluhr et al., 2012]. In this way, TTP has been suggested
77 for different applications in dentistry [Kim et al., 2014].

78 Therefore, plasma is emerging as a physical treatment with microbicidal potential on
79 bacteria, parasites, fungi, spores, and viruses [Sladek, 2005; Fridman et al., 2007; Kolb et
80 al., 2008; Von Woedtke et al., 2008; Dobrynin et al, 2009; Rupf et al., 2010]. Also, TTP
81 may allow its application inside the mouth because of it is compatible with the mammalian
82 tissues, which encourages their use *in vivo* [Fluhr et al., 2012; Partecke et al., 2012;
83 Delben, 2016]. The first hypothesis to be tested in this study is that TTP have
84 antimicrobial effect on microorganisms present in biofilms formed *in situ*. Furthermore, the
85 hypothesis that plasma treatment will damage the enamel structure will be tested.

86

87 MATERIALS AND METHODS

88 *Ethical Aspects*

89 This study was approved by the Institutional Ethical Committee and all volunteers
90 gave informed consent (Sisnep Caae - 40975514.0.0000.5054). .

91

92 *Experimental design*

93 For this *in situ* experiment, a single-blind split mouth design was used in two intra-
94 oral phases of 7 days (7d) each, in which 22 volunteers wore palatal devices containing six
95 bovine enamel slabs, positioned in pair of three. At the end of each intraoral phase, the
96 device was randomly split and each half (containing three enamel slabs) was allocated into
97 one of the following treatments: Plasma (PLA); Argon flow (AIR); Chlorhexidine 0.12%
98 (CHX) or Salina solution 0.89% (SAL) as described in Fig 1. In this way, at the end of the
99 two clinical phases, all volunteers were submitted to the four different treatments (Fig.2).

100

101 Figure 1 – Description of the treatments in which the enamel slabs were allocated.

Groups	Treatment
PLA	Plasma plume scanning enamel surface during 5 min
AIR	Argon gas flow scanning enamel surface during 5 min
CHX	A drop of 50 μ L on each slab during 5 min
SAL	A drop of 50 μ L on each slab during 5 min

102

103 *Tissue-Tolerable Plasma*

104 The Tissue-Tolerable Plasma TTP source that was utilized in this study was
105 developed by the Leibniz Institute for Plasma Science and Technology (Neoplas Tools –
106 KINPen, Greifswald, Germany) and consists of a hand-held unit (length = 170 mm,
107 diameter = 20 mm, weight = 170g) connected to a high-frequency power supply (frequency
108 1.82MHz, 2–6 kV peak-to-peak, 8 W system power) for the generation of a plasma jet at
109 atmospheric pressure. The hand-held unit has a pin-type electrode (1 mm diameter)
110 surrounded by a 1.6 mm quartz capillary. An operating gas consisting of argon at a flow
111 rate of 5 standard liters per minute (slm) was used. The plasma plume emerging at the exit
112 nozzle is about 1.5 mm in diameter and extends into the surrounding air for a distance of
113 up to 10mm [Delben, 2016]. The gas flow/TTP plume was targeted to all surface of enamel
114 slabs, and a surface scanning were performed manually by a single operator.

115

116 *Specimen preparation*

117 Bovine teeth were used to perform this *in situ* study. The teeth were stored in 0.01%
118 (v/v) thymol solution at 4°C for 30 days until be used [Cury et al., 2000]. Enamel slabs with
119 4 x 4 x 2 mm were obtained using a water-cooled diamond saw and a cutting machine
120 (IsoMet Low Speed Saw; Buehler, Lake Bluff, IL, USA). The adjustment of the enamel to
121 obtain flat plates was done with the aid of a low-speed polishing machine and 320 grit
122 paper (Carbimet Paper Discs; Buheler-met® II, USA), under water-cooling. Afterwards,
123 the specimens were polished using three different silicon carbide waterproof papers (320,
124 600, and 1,200-grit) as well as polishing cloths with 1µm diamond paste (Buehler®, Illinois,
125 USA).

126

127 *Microhardness analysis*

128 Surface Microhardness (SMH) was performed using a Knoop indenter with a 50g
129 load for 5s in a Future-Tech FM Microhardness Tester coupled to the FM-ARS software
130 (Future-Tech Corp., Tokyo, Japan). Initial SMH measurements were made in the center of
131 the enamel surface making one row of five indentations. For selection purposes, enamel
132 slabs with SMH values ranging from 272- 440 Knoop hardness number were selected in a
133 total of two-hundred and sixty-four slabs that were used in this experiment [Meredith et al.,
134 1996]. After the intra-oral phase and treatments, SMH measurements were repeated
135 spaced at 100 µm on the side right of the five baseline indentations. Also, the percentage
136 of surface microhardness change (%SMC) was calculated ($\%SMC = \frac{SMH \text{ after treatment} - SMH \text{ baseline}}{SMH \text{ baseline}} \times 100$).
137

138

139 *In situ palatal devices*

140 After baseline SMH, the slabs were autoclaved (121 °C, 15 min) [Yamamoto et al.,
141 2005] and stored in 100% humidity until being inserted into the palatal appliances. For
142 each subject, two acrylic palatal devices were prepared, in which two cavities (18 x 6 x 3
143 mm) were made on the left and right sides; and three slabs were attached with wax in
144 each cavity. In order to allow biofilm accumulation, and to protect it from mechanical
145 disturbance, a plastic mesh was positioned on the acrylic resin, leaving a 1 mm space
146 from the slab surface [Hara et al, 2003].

147

148 *In situ study Population*

149 Twenty-two healthy volunteers (16 women and 6 men), aged from 19 to 34 years,
150 able to comply with the experimental protocol, were selected to participate in this study. All

151 participants received oral and written instructions about the experimental design. The
152 inclusion criteria were normal salivary flow rate, normal buffering capacity of saliva and *S.*
153 *mutans* colony-forming units (CFUmg⁻¹) in biofilms of at least 10⁵ after 36 h of oral hygiene
154 suspension. Exclusion criteria included active caries lesions, use of antibiotics within the
155 past 3 months prior to the study, and the use of fixed or removable orthodontic devices.

156

157 *In situ* biofilm formation

158 During the lead-in period (7d) and throughout the clinical 2 phases (7d each), the
159 volunteers brushed their teeth with a fluoridated dentifrice [Sorriso Super Refrescante – a
160 calcium carbonate based dentifrice, 1,450 µg fluoride (F) g⁻¹, as monofluorophosphate
161 [MFP, Colgate-Palmolive, São Paulo, SP, Brazil]. Also, the volunteers received oral and
162 written instructions to wear the appliances at all times, including at night. They were
163 allowed to remove the appliances only during meals, when consuming acid drinks, and
164 when performing oral hygiene. When removed, the devices were kept moist in plastic
165 boxes to keep the bacterial biofilm viable [Cury et al., 2000]. The cariogenic challenge was
166 provided by the volunteers who dripped a 10% sucrose solution onto all the enamel slabs,
167 10 times a day, according to a predetermined schedule (at 08:00, 09:30, 11:00, 12:30,
168 14:00, 15:30, 17:00, 18:30, 20:00, and 21: 30 h) [Duggal et al., 2001]. Before replacing the
169 palatal appliance in the mouth, a 5-min waiting time was standardized to allow diffusion of
170 the sucrose into the dental biofilm. Brushing with the dentifrice was performed three times
171 a day, after mealtimes when the volunteers habitually carried out their oral hygiene
172 procedures. The appliances were brushed extra-orally, except for the slab area, to avoid
173 disturbing the biofilm. All volunteers consumed fluoridated water (0.70 mg F l⁻¹), and no
174 restriction was made with regard to the volunteers' dietary habits.

175

176 *Treatment of in situ* biofilms

177 Microbiological analyses of the oral biofilm were performed on the 7th day of the
178 experiment immediately after performing the treatments. The distribution of treatments on
179 the palatal device in each intra-oral phase was determined randomly by raffle. All
180 volunteers attended to laboratory in fasting and one drop of 10% sucrose was added to
181 each slabs before the device was removed from mouth. Thirty minutes after, the plastic
182 meshes of the devices were removed with a scalpel blade (#15C), the biofilm formed *in*
183 *situ* were exposed, and the treatments with PLA, AIR, CHX or SAL were performed.
184 Biofilms were then scraped carefully and weighed using microcentrifuge tubes, to which
185 1000 µl 0.89% NaCl solution was added. To disperse the biofilms, the samples were

186 sonicated at an output of 7W (Sonifier450D, São Bernado do Campo,SP, Brazil) using 3
187 pulses of 15 s with interval of 15 s of rest on ice. Afterwards, the suspension was serially
188 diluted (1:10, 1:100, 1:1.000, 1:10.000, 1:100.000, and 1:1.000.000) in 0.89% NaCl
189 solution. In order to assess microorganism viability, samples were plated in triplicate on
190 the following culture media: mitis salivarius agar (MSA), containing 15% sucrose, to
191 determine total streptococci; MSA agar plus 0.2 units of bacitracin ml^{-1} to determine
192 *mutans streptococci* [Gold et al., 1973], rogosa agar supplemented with 0.13% glacial
193 acetic acid to assess the number of lactobacilli [Rogosa et al., 1951] and blood agar to
194 determine total microorganisms. The plates were incubated for 48 h at 37°C in a partial
195 atmosphere of 5% CO_2 . Representative colonies of *mutans streptococci*, total streptococci,
196 *lactobacilli*, and total microorganisms were counted using a colony counter, and the results
197 were expressed as colony-forming units (CFU) mg^{-1} of biofilm.

198

199 *Scanning Electron Microscopy (SEM)*

200 For SEM, samples from bovine enamel slabs rinsed with distilled water, were
201 vacuum dried for 24h and then mounted on a SEM stub (aluminum discs), fixed with
202 double sided adhesive carbon tape, coded and mounted onto aluminium stubs with
203 Acheson silver DAG (Agar Scientific, U.K.) and then coated with a 15 nm thick layer of
204 gold, using a Polaron SEM coating unit. The specimens were then examined using an
205 SEM (Inspect™ S50, Jeol, Tokyo, Japan), operating at 20 KV and working distance
206 10mm. Images were taken at 2 levels of magnification ($\times 5000$ and $\times 10000$) in order to
207 assess for changes in surface structure and captured using an specific software (EDS
208 Software for SEM, Oxford instruments). The images were analyzed visually.

209

210 *Raman Spectroscopy*

211 The Raman spectra were acquired on a Raman spectrometer (Xplora HORIBA,
212 Kyoto, Japan). For excitation of the samples it was used a HeNe laser operating at 632.8
213 nm wavelength. The enamel slab sample was placed onto a substrate, the laser beam was
214 focused on the sample surface using a microscope (OLYMPUS, Japan) with lens of 10x
215 and numerical aperture 0.75 forming a spot approximately 4 μm over the surface of the
216 sample, and three points were chosen for Raman measurement with an exposure time of
217 30 s. The first point was located in the central region of the dental slab, and the others
218 were located to the right and to the left of this first point. The distance between the points
219 was 1 mm. The Raman system was calibrated with a silicon semiconductor using the
220 Raman peak at 521 cm^{-1} . All spectra were taken and collected in the region from 200 to

221 3600 cm⁻¹ and allowed a characterization of both mineral content (hydroxyapatite) and
222 organic (essentially collagen) constituents. The curve was identified for each band using
223 an OriginPro 8.6 32 bit software system (Operating System: 7, Copyright 2012 by
224 OriginLab Corporation, Northampton:MA. USA).

225

226 *Statistical analysis*

227 The sample size was calculated by using data from an initial study, assuming on a
228 medium effect size of 0.5, significance level 5%, and statistical power 95%, it was found
229 that the study required 16 participants. Twenty- two participants were screened to ensure
230 that at least 16 subjects would successfully complete the study. Each participant wore an
231 upper removable appliance containing six enamel slabs. The study consisted of two
232 phases and each phase lasted for 7-days. Therefore, a total number of 264 enamel slabs
233 were required for the whole study.

234 The normality distribution of the data was checked using the Kolmogorov-Smirnov
235 statistical test. The mean and the standard deviation (SD) of the numbers of surviving
236 microorganisms for each treatment were calculated. Colony-forming units were
237 transformed into log 10 colony-forming units in order to reduce variance heterogeneity. To
238 determine the differences between test and control values, the unpaired one-way analysis
239 of variance followed by a Holm-Sidak test or non-parametric Kruskal-Wallis followed by a
240 Dunn's Multiple Comparison Test were used when appropriate. Paired- t test was used to
241 compare baseline and after intraoral phase SMH. Differences among the experimental
242 periods in relation to %SMC were tested by Kruskal-Wallis One Way Analysis of Variance
243 on Ranks. For Raman in order to normalize measurements and allow their comparison,
244 the band height parameter was used. The mean of the peaks height were compared using
245 test one-way analysis of variance (ANOVA). Significance level was set at 5% ($p < 0.05$)
246 using the software SigmaPlot 11.0 (La Jolla, CA, USA).

247

248

249 **RESULTS**

250

251 *Microhardness analysis*

252 The results for enamel surface microhardness before and after treatment and also
253 the percentage of microhardness change can be found in table 1. The comparison of
254 different treatments showed no statistical significant difference among them ($p= 0.36$).

255

256 *Microbiological viability*

257 All volunteers showed normal patterns in the salivary tests with mean values of 1.56
258 ml/min salivary flow rate, normal buffering capacity (pH= 5.13) and 7.37×10^6 CFU ml⁻¹ of
259 *mutans streptococci* in biofilms formed after 36 h of oral hygiene suspension. The effect of
260 plasma treatment on viability of *in situ* biofilms can be found on Figure 3. Plasma treatment
261 showed a significant reduction for total microorganism (p<0.001), total streptococci (p=
262 0.037), and *mutans streptococci* (p= 0.004) counts. *Mutans streptococci* counts were also
263 reduced by argon gas treatment. Thus, plasma treatment did not demonstrate influence on
264 lactobacilli viability (p= 0.497). For the other tested microorganisms there were no
265 statistical difference among saline solution, argon gas and CHX treatments. The
266 percentage of viable *mutans streptococci* related to total streptococci was 7.86% in plasma
267 treatment, 10.23% in argon treatment, 15.34% in saline group and 8.10% in chlorhexidine
268 treatment.

269

270 *Scanning Electron Microscopy (SEM)*

271 SEM analysis revealed smooth and homogenous surface topography of enamel at
272 both x5000 (Figure 4: 1A, 2A, 3A and 4A) and x10000 whereas in region enamel the
273 demineralized showed irregularities and stepped lamination appearance (Figure 4: 1B, 2B,
274 3B, and 4B) magnification. No difference was observed among the surfaces of different
275 treatment groups.

276

277

278 *Raman Spectroscopy*

279 The average Raman spectra for the four treatment groups in the region of 200-
280 3600 cm⁻¹ are shown in Fig. 5. All spectra were normalized based on the 960 cm⁻¹
281 phosphate peak, which was the most intense peak. The region spanning from 240 to 1.045
282 cm⁻¹ was characteristic of phosphate and carbonate groups and representative of the
283 mineral phase of enamel and the region spanning from 1448 to 3080 cm⁻¹ was
284 characteristic of C-H bond stretching and amide bending vibrational modes from proteins
285 in the organic matrix of the enamel.

286 The band in the range of ν_1 (240-330 cm⁻¹) represents the carbonate vibration,
287 bands at ν_2 (582 cm⁻¹), ν_3 (960 cm⁻¹), ν_4 (1045 cm⁻¹), represent the phosphate vibrations
288 in hydroxyapatite, and bands ν_5 (1448 cm⁻¹), ν_7 (1653 cm⁻¹) amide bending vibrational
289 modes from proteins in the organic matrix of the enamel and ν_6 (1465 cm⁻¹), ν_8 (2943 cm⁻¹)
290 ¹) representing C-H.

291 In Fig. 06, Raman-spectra from enamel slabs with treatment plasma (in black),
292 argon flow (in red), 0.89% NaCl saline solution (in blue) and chlorhexidine (in green) are
293 shown with similar vibrational modes. Although in the peaks intensity of the SAL group
294 was higher than the other groups, no statistically significant differences were detected in
295 the peak intensity observed for all bands in all tested groups ($p= 0.123$).
296

297 **DISCUSSION**

298 The main finding of the present study is that Tissue-Tolerable Plasma was effective
299 against mature oral biofilm formed *in situ*, being more effective in reduce bacterial viability
300 than chlorhexidine, a well-known antimicrobial substance. Additionally, this is the first *in*
301 *situ* study evaluating the antimicrobial effectiveness of Tissue-Tolerable Plasma treatment
302 on oral biofilms. The oral biofilm containing pathogenic bacteria communities is one of the
303 major factor associated with dental caries [Guo et al., 2015]. Also, microorganisms
304 growing in biofilms may be up to 1000 times more resistant to antimicrobial agents than
305 their planktonic counterparts [Costerton et al., 1999; de Melo et al., 2013]. In this way, the
306 interest in new strategies to effectively inactivate pathogenic bacteria in oral biofilms has
307 emerged in the scientific community and the use of the Tissue-Tolerable Plasmas are one
308 of these new therapies because of its effectiveness against oral microorganisms [Gorynia
309 et al., 2013; Blumhagen et al., 2014; Sladek et al., 2014].

310 This study compared the antimicrobial effect of several treatments on oral biofilms.
311 CHX solution is a golden standard to inactivate or prevent dental plaque formation
312 [Matthews, 2011] when compared to other chemical agents used in dentistry [Filoche et
313 al., 2005]. However, a 0.1% CHX solution seems to be inefficient against mature oral
314 biofilms [Vitkov et al., 2005]. The main advantage of using CHX is its wide antimicrobial
315 spectrum, acting on both Gram-positive and Gram-negative microorganisms and its
316 prolonged and continuous effect even in the presence of blood and other body fluids
317 [Rosenthal et al., 2004]. However, the prolonged use of CHX can cause mucous peeling,
318 stains on the teeth, alterations in the sense of taste, compromising of the wounds healing
319 and reduction of fibroblast adhesion to radicular surfaces [Zheng and Wang, 2011]. Thus a
320 potential antimicrobial adjuvant alternative to CHX with less side-effect would be of great
321 value in dentistry. In our study, plasma treatment showed better results than CHX in
322 reducing total microorganism, total streptococci and *mutans streptococci*, similarly found

323 by the Koban et al. [2010] *in vitro* using TTP treatment against oral biofilms formed on
324 titanium discs.

325 In our study, complex *in situ* multispecies biofilms were significantly affected by TTP
326 after 5 min treatment. Although we did not investigate the mechanism of action of TTP on
327 bacterial species, there are many possible mechanisms that may explain its bactericidal
328 activity, such as electron bombardment of cell membranes, charge accumulation, chemical
329 reactions such as oxidation, destruction of nucleic acids by ultraviolet radiation, and
330 ablation of the cell membrane [Laroussi, 2005]. In all cases, the site of action for the
331 plasma deactivating mechanisms is either at the cell membrane or the DNA. Argon plasma
332 acts via a complicated mechanism that includes a synergetic action of reactive species of
333 different kinds, including ionized argon gas molecules [Shimizu et al., 2008]. TTP reactive
334 particles produce a general mechanical effect on the surface of living organisms, which
335 has been called etching [Lerouge et al., 2000a; Moisan et al., 2001; Moreau et al., 2008].

336 Etching is due to the reaction of highly reactive gas radicals with organic materials,
337 generating products that disrupt membrane surface. It may cause perforations in the
338 membranes of microorganisms, which, in turn, remove the obstacle to secondary reactive
339 species that might be formed in the medium. The effectiveness of etching depends on
340 plasma composition [Lerouge et al., 2000b]. Park et al. [2014], related that it is possible
341 that several components work together to produce a synergistic effect rather than a single
342 component contributing to the sterilization. TTPs may produce a large amount of reactive
343 oxygen species (ROS) when it passes through air, and in particular, high levels of OH are
344 generated when plasma reacts with water or tissue fluid. It is well known that OH
345 effectively kills bacteria. Furthermore, the half-life of plasma-generated ROS is very short,
346 and hence, its retention in the oral cavity is short and less likely to induce harmful effects
347 on tissues.

348 The TTP treatment was more effective to reduce total microorganisms than
349 chlorhexidine treatment. Ermolaeva et al. [2011] suggested that, in general, TTP argon
350 plasma is more effective against Gram-negative than Gram-positive bacteria because of
351 the differences in cell-wall structure. In our study, we did not test plasma treatment in
352 gram-negative bacteria disconnected of other microorganism, but our oral biofilms contain
353 both gram-negative and positive bacteria and the treatment was effective in reduce them.
354 So, further experiments are needed to evaluate the effectiveness of plasma treatment on
355 gram-negative bacteria.

356 As observed to total microorganisms, the counts of total streptococci after TTP
357 treatment was inferior than observed to chlorhexidine. The degree of inhibition is probably
358 related to the thickness of the biofilm once thicker biofilm, such as those formed in the
359 presence of sucrose [Roberts et al. 2002], would present a greater challenge for the
360 penetration of plasma free radicals [Sladek and Stoffels, 2005; Vleugels et al. 2005]. This
361 could also inhibit the antibacterial activity of the TTP, killing cells only at the surface of
362 biofilms and inducing a sublethal response to cells attached to the substrate [Sladek and
363 Stoffels 2005]. Also, the partial antimicrobial effect achieved in our study may be explained
364 by characteristics of different bacteria present in biofilms that turn them more resistant to
365 antimicrobial treatments. In this way, Gorynia et al., [2013] tested argon plasma in *S.*
366 *sanguinis* biofilms and found that TTP was not effective on this bacteria which may be
367 attributed to its fast metabolic ratio and also to its ability of attaches to surfaces 10 to 100
368 times stronger than *S. mutans*, *S. mitis* and *S. salivarius*, generating more stable biofilms
369 [Rosan et al., 1982].

370 Despite the majority of the studies test TTP treatment against planktonic cultures,
371 Goree et al. [2006] investigated the use of a plasma needle in *mutans streptococci*
372 colonies and observed that TTP was able to kill bacteria after 10 seconds of treatment.
373 They concluded the plasma could provide an attractive alternative treatment for dental
374 clinic. Yang et al. [2011] and Blumhagen et al. [2014] used the TTP argon plasma against
375 *mutans streptococci* and *Lactobacillus acidophilus* and observed that TTP was effective in
376 reducing the number of *S. mutans* after 11-15 sec and that results were dependent of the
377 bacterial supporting media. Similar results were also observed on monospecies biofilms
378 with different types of plasma source such as helium and oxygen gas [Sladek et al., 2004;
379 Yamazaki, 2011]. Also, the percentage of viable cariogenic *mutans streptococci* related to
380 total streptococci was almost half in TTP treatment compared to negative control.

381 In our study there was not observed statistically significant reductions on viability of
382 *Lactobacilli sp* among the tested treatments. Yang et al., [2011] found that longer plasma
383 treatment was required for deactivating *L. acidophilus* than used to kill *S. mutans*. The
384 sterilization mechanisms of TTP indicate that bacterial sizes and structure would affect the
385 plasma effectiveness and efficiency in bacterial deactivation. The bigger cell size of *L.*
386 *acidophilus* (~ 1 × 3 µm in diameter) would receive less free radicals per unit of cell making
387 than harder to kill than the smaller *S. mutans* (~ 1 µm in diameter). In order to achieve the
388 same intensity of injection plasma for a single cell, under the same plasma conditions,

389 several minutes of exposure time were needed to kill *L. acidophilus*, while only tens of
390 seconds of exposure time was needed for *S. mutans*.

391 In the present study, enamel demineralization was observed after 7 days of plaque
392 accumulation at high frequency of exposure to sugar (Table 1). It was observed a
393 reduction in superficial enamel microhardness (SMH) due to the cariogenic challenger to
394 which enamel blocks were submitted. The SMH is considered a very sensitive method of
395 evaluating early caries lesion [Zero, 1995]. Tenuta et al. (2003) suggest that it takes
396 around 3-4 days for dental plaque to manifest its cariogenicity on dental substrate but this
397 period could be shorter for bovine enamel [Featherstone and Mellberg, 1981]., Thus, the
398 mineral loss found in our study is similar to those founded for human enamel by other
399 authors [Park et al., 2004]. Also, the treatment with argon plasma, argon flow, 0.12 %
400 chlorhexidine, and 0.89% NaCl solution had no effect on SMC%, suggesting that the
401 plasma treatment do not interfere in enamel hardness under tested conditions. These
402 results indicated that plasma treatment did not induce damage in the enamel surface
403 despite enamels slabs have suffered cariogenic challenge. Chen et al. [2013] also did not
404 observed surface modification of several dental substrates submitted to by Tissue-
405 Tolerable Plasma treatment.

406 The raman spectroscopy allows a molecular analysis of mineralized dental tissues.
407 The information is provided as curves representing the intensity of the signal according to
408 the frequency and mathematical analyses may be performed in order to provide
409 comparative and quantitative analysis [Tramini et al., 2000]. To our knowledge, this is the
410 first study that has characterized and compared the molecular structure of the enamel
411 submitted to the plasma treatment. The reading of the slab in three different points allows
412 us to compare statistically all the treatments, however, no significant difference in mean
413 intensity of the peaks.

414 In conclusion, our results demonstrate that the argon TTP under tested conditions
415 was effective in reducing the viability of *mutans streptococci*, total streptococci and total
416 microorganism, without damage the surface of enamel.

417

418

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423

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- 657

Tables

Table1: Surface microhardness analysis of enamel slabs according to the treatment (mean \pm SD).

Treatment	SMH		%SMC
	Baseline	After intraoral phase	
Plasma	324.03 \pm 31.82a	210.98 \pm 90.53b	-34.99 \pm 21.92A
Argon flow	312.87 \pm 26.90 a	230.81 \pm 51.37 b	- 26.32 \pm 09.77A
NaCL 0,89%	318,35 \pm 30,61 a	193.11 \pm 87.99 b	-39.06 \pm 21.79A
Chlorexidine	315,88 \pm 28.46 a	212.45 \pm 70.03 b	-32.49 \pm 14.78 A

Different letters indicate statistically significant differences ($p < 0.05$). Capital letters compare the columns; low case letters compare the lines. SMH = surface microhardness; SMC = surface microhardness change.

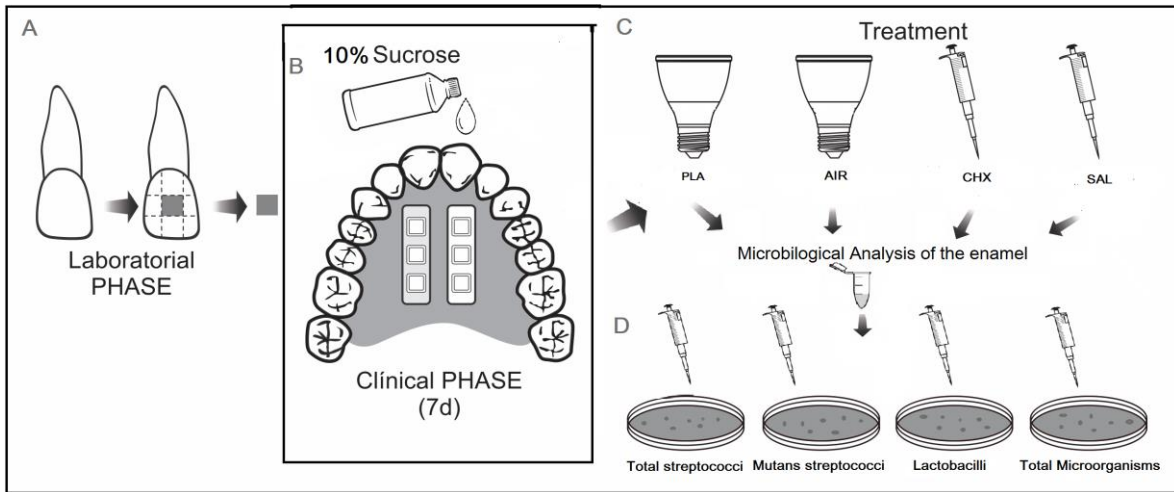


Figure 2 – Experimental Design. In (A) enamel slabs from bovine teeth stored in 0.01% thymol. (B) Clinical phase to provide a cariogenic challenge. (C) Each slab following treatments for 5 min: PLA, AIR, CHX and SAL. (D) Biofilm samples plated in triplicate in MSA, MSB Agar, Rogosa Agar and in Blood Agar.

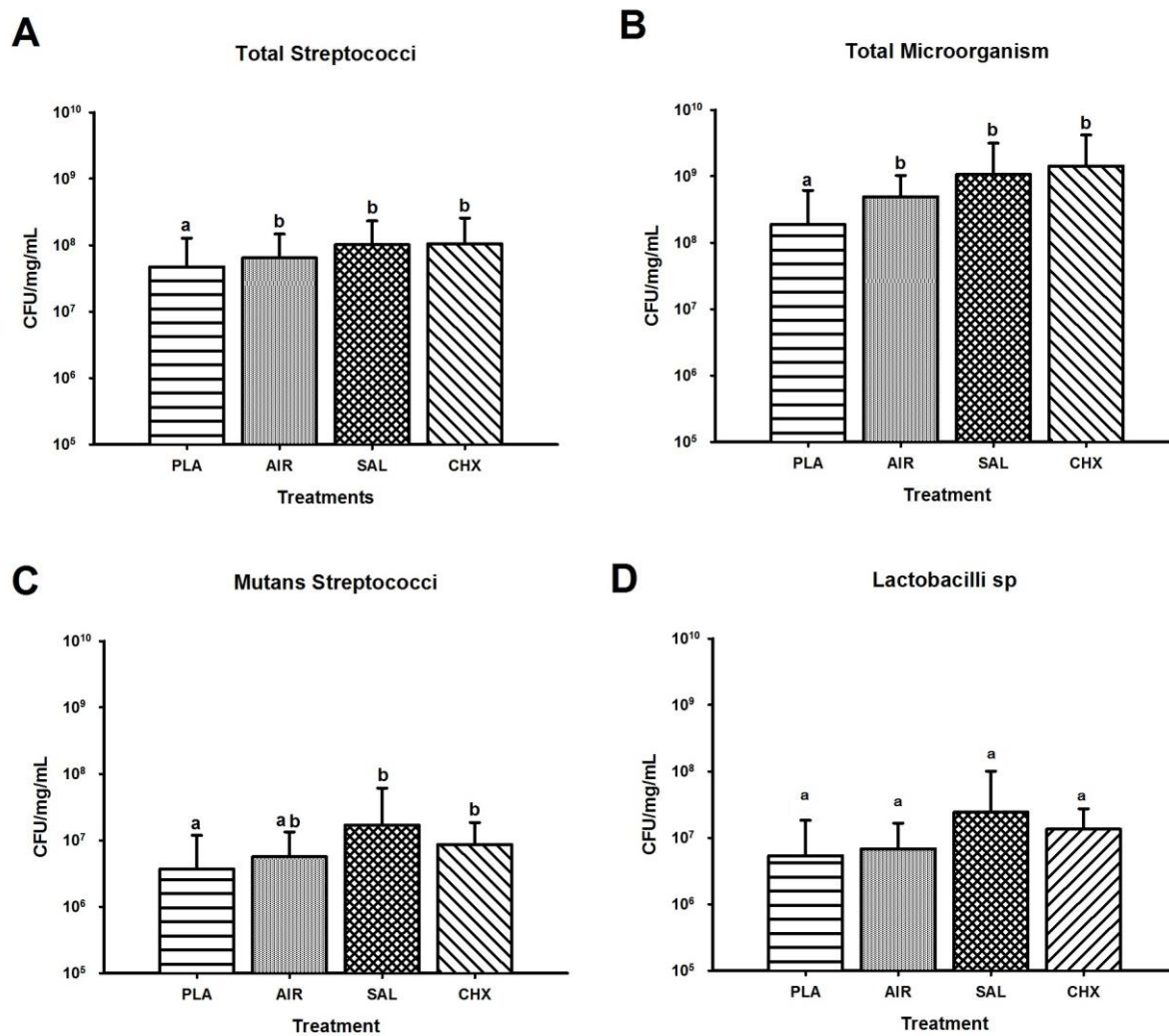


Figure 3 – Effects of the treatments PLA, AIR, SAL and CHX on viability of (A) total streptococci, (B) total microorganisms, (C) *mutans streptococci* and (D) *lactobacilli sp.* Data represent the mean values and error bars represent standard deviations. Data followed by different letters differ statistically ($p < 0.05$).

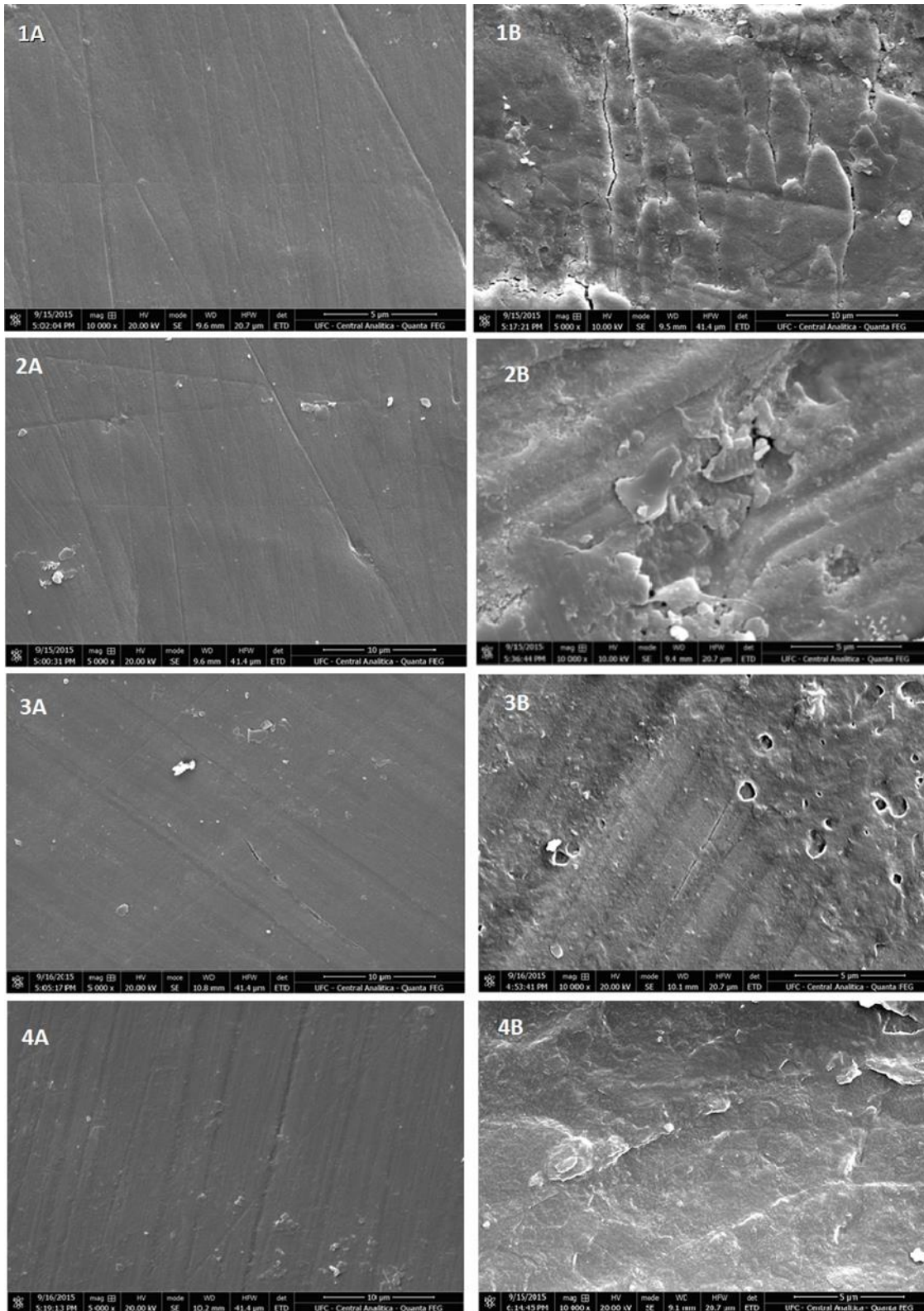


Figure 4 – SEM analysis respectively to PLA, AIR, CHX, SAL treatments at x5000 (1A, 2A, 3A and 4A) and x10000 (1B, 2B, 3B, and 4B) region desmineralised the enamel.

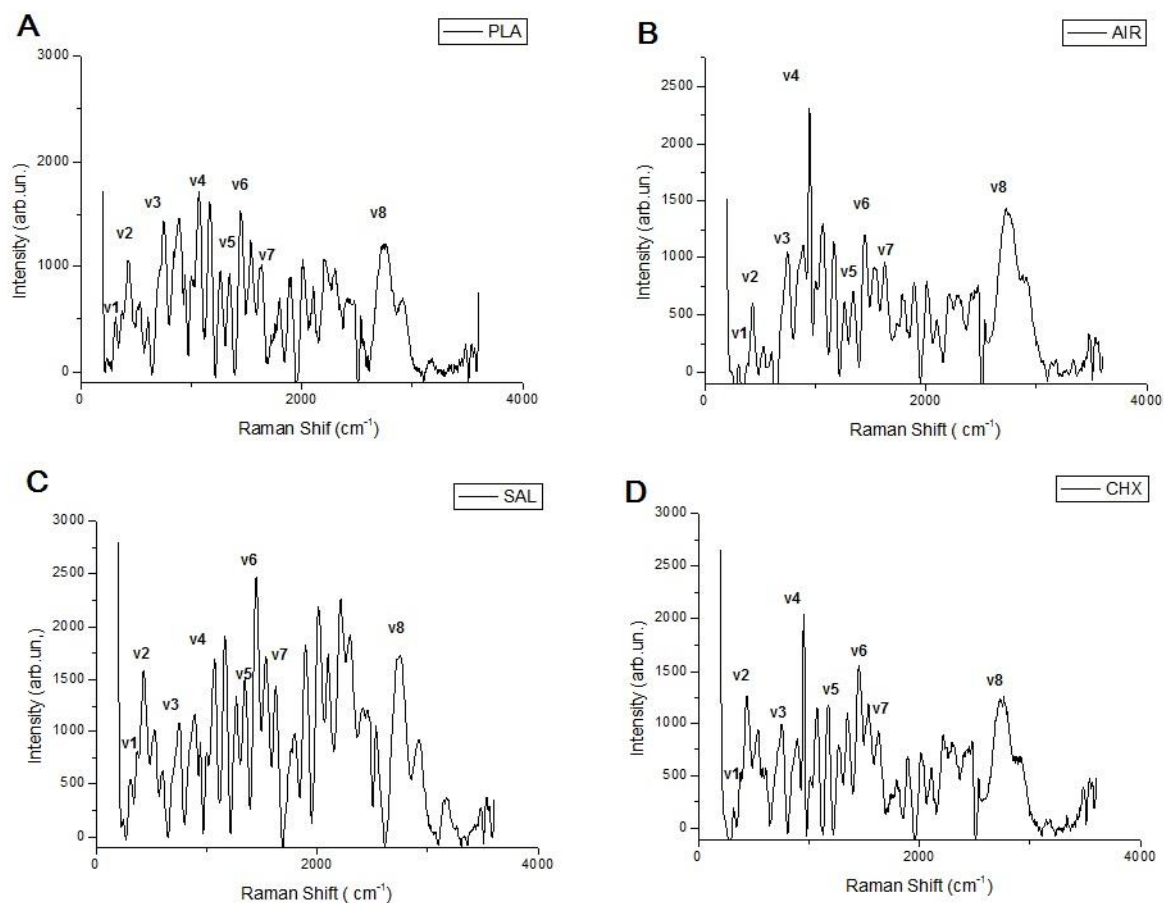


Figure 5: Raman band at $v_1=324\text{ cm}^{-1}$ characteristic of carbonate vibration, $v_2=582\text{ cm}^{-1}$, $v_3=960\text{ cm}^{-1}$, $v_4=1045\text{ cm}^{-1}$ characteristic of phosphate vibration, $v_5=1448\text{ cm}^{-1}$, $v_6=1465\text{ cm}^{-1}$, $v_7=1653\text{ cm}^{-1}$ and $v_8=2943\text{ cm}^{-1}$ phase organic. In (A) PLA; (B) AIR; (C) SAL; (D) CHX treatments.

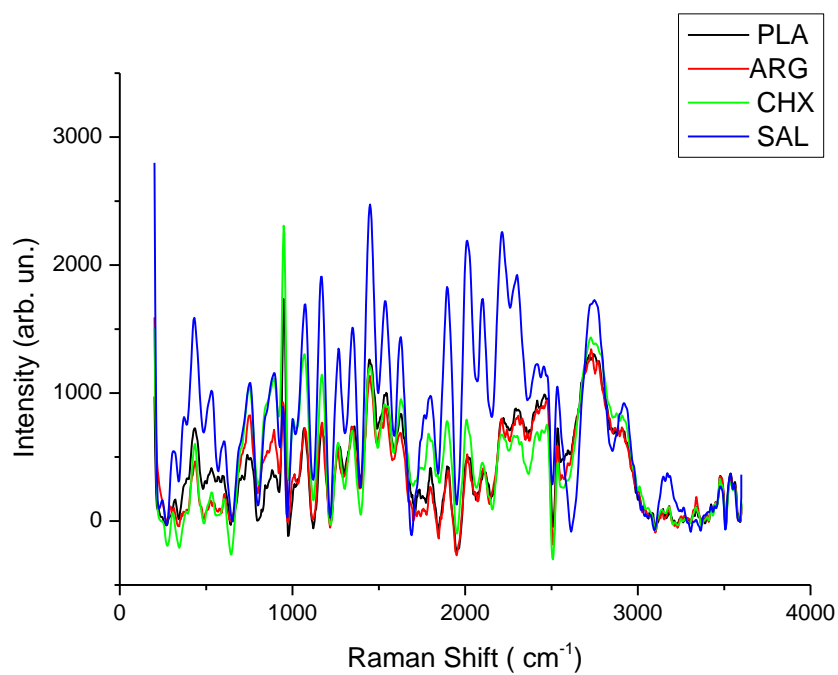


Figure 6 – Raman spectra of treatments plotted together. Treatments PLA (in black), AIR (in red), SAL (in blue) and CHX (in green).

4 CONCLUSÃO

Nas condições testadas o Plasma de Baixa Temperatura foi eficaz na redução da viabilidade de *Streptococcus mutans*, estreptococos totais e microrganismos totais, sem alterar a estrutura do esmalte sob biofilme irradiado.

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ANEXO A – APROVAÇÃO DO COMITÊ DE ÉTICA

UNIVERSIDADE FEDERAL DO
CEARÁ PROPESQ



PARECER CONSUBSTANCIADO DO CEP

DADOS DO PROJETO DE PESQUISA

Título da Pesquisa: Atividade do plasma de baixa temperatura em biofilmes orais formados in situ

Pesquisador: Karla Shangela da Silva Alves

Área Temática:

Versão: 2

CAAE: 40975514.0.0000.5054

Instituição Proponente: UNIVERSIDADE FEDERAL DO CEARA

Patrocinador Principal: Financiamento Próprio

DADOS DO PARECER

Número do Parecer: 1.000.400

Data da Relatoria: 26/03/2015

Apresentação do Projeto:

Projeto de doutorado de Karla Shangela da Silva Alves sobre a utilização do plasma de baixa temperatura (PBT) na terapia anti-placa e anti-cárie, já que esta tecnologia provoca destruição da matriz extracelular de bactérias e, estudos preliminares demonstraram a sua eficácia sobre biofilme oral maduro. Serão selecionados vinte voluntários (estudantes do curso de Odontologia da FFOE-UFC) que receberão um dispositivo palatino intra-oral fabricado com metal, esmalte e tela para retenção de bactérias e formação de biofilme. Após 7 (sete) dias, estes dispositivos serão removidos e tratados, em laboratório, com terapia PBT. Cada amostra terá uma área irradiada e uma outra não, esta última, considerado o controle. Após o tratamento, os espécimes serão analisados quanto à viabilidade bacteriana, propriedades bioquímicas da matriz do biofilme, determinação das possíveis alterações da superfície do esmalte e caracterização molecular da população microbiana dos biofilmes tratados pela técnica do PCR-DGGE. A análise de Variância e o teste Tukey serão utilizados tendo o nível de significância estabelecido em 5%.

Objetivo da Pesquisa:

Objetivo Primário:

Elucidar e aperfeiçoar uma abordagem única para um agente anti-placa, usando os efeitos sinérgicos do PBT de (i) destruir a matriz extracelular do biofilme maduro e (ii) a ação antimicrobiana, entretanto sem prejudicar o esmalte.

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ANEXO B – NORMAS DA REVISTA A SER SUBMENTDIDO

KARGER



Caries Research

Contents: all years

Guidelines for Authors

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Aims and Scope

'Caries Research' is an international journal, the aim of which is to promote research in dental caries and related fields through publication of original research and critical evaluation of research findings. The journal will publish papers on the aetiology, pathogenesis, prevention and clinical control or management of dental caries. Papers on health outcomes related to dental caries are also of interest, as are papers on other disorders of dental hard tissues, such as dental erosion. Aspects of caries beyond the stage where the pulp ceases to be vital are outside the scope of the journal. The journal reviews papers dealing with natural products and other bacterial inhibitors against specific criteria, details of which are available from the Editor.



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